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Review article

Engineering DNA vaccines against infectious diseases

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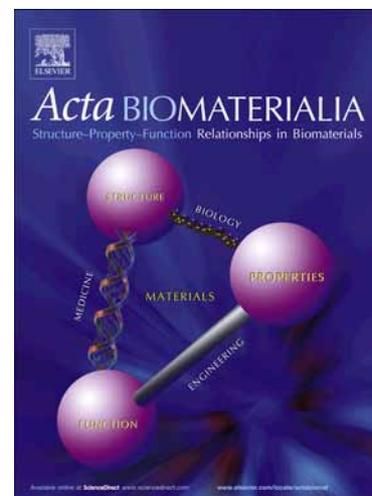
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Abstract

Engineering vaccine-based therapeutics for infectious diseases is highly challenging, as trial formulations are often found to be nonspecific, ineffective, thermally or hydrolytically unstable, and/or toxic. Vaccines have greatly improved the therapeutic landscape for treating infectious diseases and have significantly reduced the threat by therapeutic and preventative approaches. Furthermore, the advent of recombinant technologies has greatly facilitated growth within the vaccine realm by mitigating risks such as virulence reversion despite making the production processes more cumbersome. In addition, seroconversion can also be enhanced by recombinant technology through kinetic and nonkinetic approaches, which are discussed herein. Recombinant technologies have greatly improved both amino acid-based vaccines and DNA-based vaccines. A plateau of interest has been reached between 2001 and 2010 for the scientific community with regard to DNA vaccine endeavors. The decrease in interest may likely be attributed to difficulties in improving immunogenic properties associated with DNA vaccines, although there has been research demonstrating improvement and optimization to this end. Despite improvement, to the extent of our knowledge, there are currently no regulatory body-approved DNA vaccines for human use (four vaccines approved for animal use). This article discusses engineering DNA vaccines against infectious diseases while discussing advantages and disadvantages of each, with an emphasis on applications of these DNA vaccines.

Keywords: DNA vaccine; immune response; infectious disease; kinetics; vaccine

1. Introduction

Infectious diseases are caused by a variety of microorganisms including bacteria and viruses and can often lead to a decrease in the quality of life and increased (risks of) mortality. In 2016, 1.6 million people died due to human immunodeficiency virus (HIV) alone. The infectious disease burden can be delineated using disability-adjusted life years (DALYs), which were listed by the World Health Organization (WHO) as a number of the top contributing issues. With regard to what was infectious disease related, the DALYs for lower respiratory infectious diseases, HIV/AIDS, and tuberculosis were 1939, 855, and 763 per 100,000 and were ranked as 2nd, 11th, and 12th, respectively, in 2015 [1]. Various therapeutic and preventative interventions have been used to combat infectious diseases. Vaccination in particular has played a critical role in preventing, treating, and even eradicating diseases (i.e., smallpox). Poliomyelitis or polio is another deadly infectious disease that mainly affects children. Inactivated poliovirus and oral poliovirus are two types of vaccinations that helped reduce polio by 99% worldwide and 80% of population worldwide live in polio-free regions [2, 3]. As of 2016, inactivated poliovirus vaccine immunizations have helped to globally eradicate wild poliovirus type 2 serotype.

Polio vaccines remain effective despite the evolution of the virus because an antigen was selected against a conserved region. However, other pathogens with antigen hypervariability vaccine efficacy will be limited. DNA vaccines can be used to overcome this challenge, as the engineered DNA can encode specific antigens. DNA recombinant-based subunit vaccines have enhanced stability for transportation and storage in comparison to traditional protein-based vaccines. There is a greater control over the risks of using DNA vaccines; therefore, DNA vaccines are

considered in some aspects to be safer. Because of this, DNA vaccines can have potentially greater utility for immunocompromised patients. However, there are remaining issues that must be resolved for enabling DNA vaccines to be clinically translated for human use. The main remaining issue is the lack of immunogenicity associated with DNA vaccines. The current state of DNA vaccines is discussed within this review article.

More specifically, this review discusses recombinant DNA subunit vaccines, mechanisms of internalization and processing, the engineering of kinetics for vaccine delivery, enhancing the duration of protection through nonkinetic approaches, manufacturing and engineering DNA, the safety and stability of DNA vaccines, plasmid delivery, controlling gene expression by plasmid engineering and gene circuits, overcoming immunogenic issues of DNA vaccines, and examples of successful commercial DNA vaccine and reports our perspective on future directions in the field.

2. Recombinant DNA subunit vaccines

A brief overview of vaccine classifications is found in **Table 1**. Extensive reviews have been written containing information regarding vaccine classifications: live-attenuated vaccines [4], polysaccharide vaccines [5, 6], inactivated vaccines [7], and DNA vaccines [4-8]. **Fig. 1** shows the number of publications between 1931 and April 2018 for different types of vaccines, which can be an indicator of popularity. We report values based on PubMed results (which could be an indicator of popularity) using EndNote between 1931 and 2020, where the projected values, as indicated by an asterisk (*) for 2011-2020, were calculated by multiplying the current values by the ratio 120/87.5. DNA vaccines, in particular, show an increased number of PubMed results when compared to other vaccine types. However, the hype of DNA vaccines is dampened, thereby reaching a plateau, likely owing to difficulties in achieving sufficient immunogenic levels for protection. DNA vaccines, however, can be engineered to have effectively zero risk for virulence reversion.

For recombinant DNA subunit vaccines, a replicating vector, typically yeast or bacteria, is transformed with an engineered DNA sequence for transcription and translation and can then be administered to the patient. For instance, Hepatitis B DNA vaccine is based on different domains of hepatitis B virus surface antigen (HBsAg) and is often administered with an adjuvant to improve immunogenicity [9, 10]. DNA vaccines encode for antigens that then mainly elicit humoral immune response similar to that of natural infection [11]. Hepatitis B DNA vaccines are often administered using liposomal or cationic carriers.

DNA and protein vaccines share a major part of the production process but vary in the mechanisms elicited in the immune system (**Figs. 2 and 3**). The first step consists in inserting the gene of interest (GOI) into the plasmid vector, followed by transformation into replicating bacteria or yeast. After the replication, the recombinant protein is extracted, purified, and prepared as a vaccine. In the case of DNA vaccines, the replicating prokaryotic vector is usually disrupted and the engineered DNA is extracted and purified to produce the final vaccine. After administration to the patient, recombinant protein vaccines are internalized within the host cells and processed to antigenic peptides, which elicit CD8 T cell responses. DNA vaccine must achieve the nucleus to use the host molecular machinery to promote the transient expression of the GOI. After the transcription and translation of the GOI, it is processed to antigenic peptides, and these antigenic peptides elicit immune responses.

In the case of a DNA vaccine, the engineered DNA can be administered to the patient with or without (i.e., gene gun) a carrier. Generally, nonviral gene delivery results in transient gene expression (TGE) of the antigen of interest. DNA vaccines were introduced in the late 90s, when Wolff et al. [12] intramuscularly injected plasmid DNA (pDNA) in mice. Subsequently, Jiao et al. [13] proposed the delivery of DNA plasmid to nonhuman primates, and Ulmer et al. [14] described a vaccine against influenza using pDNA in mice. The following sections provide in-depth information about DNA vaccines: manufacturing and engineering DNA vaccines; safety and stability of DNA vaccines; kinetic control for DNA vaccine release; barriers for the delivery of pDNA vaccines; active nuclear transport for the nuclear uptake of DNA; controlling gene expression through plasmid engineering and gene circuits; techniques to overcome immunogenic issues of DNA vaccines; and the physical methods for DNA vaccine delivery in preclinical and clinical trials.

Pros: DNA vaccines have low production cost when compared to protein vaccines and enhanced stability for transportation and storage and can be administered to immunocompromised patients. Cons: low immunogenicity and may require multiple booster doses.

3. Mechanisms of internalization and processing

A vaccine is processed by three main pathways: direct somatic cell engulfment/antigen-presenting cell (APC) display (**Fig. 2(1, 5, 3)**), thus leading to MHC II-peptide display); phagocytosis of a transfected (nonviral) or transformed (viral) cell/cross-priming (**Fig. 2(1, 4, 6)**), thus leading to MHC I-peptide display); and Toll-like receptor (TLR) activation (**Fig. 2(2, 7)**). A vaccine may be taken up intracellularly by endocytosis within APCs (**Fig. 2:(1)**) [15] or interact extracellularly by the TLR2/4 pathway, thereby resulting in the expression of proinflammatory cytokines and chemokines (interleukin (IL)-8/10, TNF α) (**Fig. 2:(2)**). When nonviral gene delivery systems are used to deliver DNA vaccines, the proton sponge effect plays an important role for the pDNA to escape the endolysosomal degradation pathway (**Fig. 2:(3)**). pDNA can be either randomly encapsulated by the nuclear envelope reforming postmitosis or actively transported to the nucleus through nuclear localization signals (*i.e.*, DNA-targeted sequences – SV40 [16]). DNA vaccines may contain unmethylated CpG sequences that function as a pathogen-associated molecular pattern (PAMP) and can activate TLR9 in the endosome, eventually releasing IL-4 and interferon (IFN) α (**Fig. 2:(4)**).

4. Enhancing the duration of immune protection using adjuvants

Enhancing the duration of immune protection by nonkinetic approaches can be achieved by (1) molecular immunostimulants (*e.g.*, nucleic acids, polysaccharides, proteins, and polymers) and (2) advanced vaccine particles (*e.g.*, nanoparticles, microparticles, and virus-like particles) (**Table 2**) [17, 18].

Biopolymers – Biopolymers (*i.e.*, polysaccharides and chitosan [CS]) are widely used for medical applications and have been reported to have adjuvant action in specific applications. For example, polysaccharide-based adjuvants can also improve the immunogenicity of vaccines. CS is a known mucoadhesive and may exhibit important roles in mucosal immunization [82]. Sawaengsak et al. [19, 20] reported nanoparticles of CS combined with tripolyphosphate and hemagglutinin (HA) to induce a twofold increase in the number of splenocytes that secrete IFN γ in mice infected with the influenza virus when compared with a nonadjuvanted HA vaccine. Gordon et al. [21, 22] reported that inulin-based adjuvants (Advax®) elicit efficient immune responses against hepatitis B (phase I). At least a fourfold increase in seroprotection and CD4 T-cell responsiveness was observed for subjects immunized with Advax® when compared to HBsAg alone. However, biopolymers have difficulties to control drug release owing to their solubility in water. For example, a report comparing pectin content demonstrated that higher pectin content resulted in increased erosion, thus leading to faster drug release; on the basis of the type of application, this concept can be an advantage or disadvantage depending on the length scale of drug release desired [23]. The reported pectin/amylose formulations released ~50%-100% of the drug within a 4 h timeframe in a gastrointestinal context.

Polymers – Relatively nontoxic and degradable (*i.e.*, through hydrolysis of esters or amidolysis of amides) polymers such as poly(anhydride) (PA), poly-*N*-isopropyl acrylamide (PNIPAAm), and PLGA have also found applications in vaccines. Tamayo et al. [24] reported the recognition of PA nanoparticles by TLR2/4/5, thereby eliciting CD8⁺ T cell responses and Th1 polarization in mice. Wafa et al. [25] showed that the polymeric structure affects the intensity of the CD8⁺ T cell response and increased the protective duration. PA nanoparticle-based vaccines were recently employed for immunizing against swine influenza within pigs [26] and against H5N1 influenza [27]. Shakya et al. [28] discussed the use of PNIPAAm combined with collagen type II as a polymeric adjuvant to reduce the risk of triggering autoimmune responses.

Several studies describe the enhanced immunogenicity due to the adjuvant properties of PLGA in comparison to nonadjuvanted antigen priming for subunit vaccines (recommended review article [29]). The size of PLGA particles (*i.e.*, nano- or microparticle), as well as the monomeric L:G ratio played a crucial role in modulating immunogenicity [30]. Li et al. [31] described an increase in Th1 cytokine expression (IFN γ and IL-17) to their pertussis toxoid vaccine by employing dual-range-sized particles ranging from 200 to 300 nm and 5 μ m with a monomeric ratio of 50:50. Another example is that of Cruz et al. [32], who reported an increased T-cell response by employing PLGA nanoparticles (50:50 L:G) for encapsulating and delivering a protein vaccine.

Molecular adjuvants for DNA vaccines – Ligands against TLRs, TLR-3 and TLR-9, have been shown to improve immune response [33]. Cytokines such as interleukin (IL)-2, IL-12, and IL-15 encoded in plasmids have also shown to enhance immunogenicity [34, 35]. Immune signaling molecules like TRIF and HMGB1 can also be encoded by the plasmid and have been successfully used as adjuvants along with DNA vaccines [36]. Genetic knockdown of genes, like PD-ligand 1 known to counteract DNA vaccines, using shRNA or siRNA has also shown to be effective adjuvants

for DNA vaccines [37]. For further information with regard to adjuvants that are specifically used along with DNA vaccines, please refer to the following extensive review articles by Li et al: [38] and by Saade F. and Petrovsky N.[36].

Pros: Similar to kinetic approaches, nonkinetic methods can also be used to achieve long-term and enhanced immune responses. Cons: adjuvants that are commonly used including alum and calcium salts can cause severe inflammation and are not compatible with, or advantageous for, certain antigens [39].

5. Manufacturing and engineering DNA vaccines

With continual improvements in DNA sequencing technology, we can better understand key conserved sequences that can be transcribed and translated into antigens and discover or engineer sequences that may be used for protection (*i.e.*, TSOL18 [40-42]). Nucleic acid code can be mass produced by DNA recombinant technology, and these codes can be directly delivered and subsequently processed and displayed by APCs for eventual seroconversion by the patient's own transcription and translation machinery. Furthermore, peptides or proteins or subunits thereof can be mass produced in cells (*i.e.*, *E. coli* and yeast) by DNA recombinant technology for manufacturing DNA vaccine.

Engineering and manufacturing DNA vaccines involve multidisciplinary fields such as molecular biology/biochemistry, separation techniques, and material science. A GOI can be inserted into a self-replicating organism (bacteria or yeast). A circular pDNA is usually used as the DNA cloning vector, which can then be extracted from the replicating organism and chemically purified [43]. The pDNA can be engineered to be expressed in bacteria (*i.e.*, *Escherichia coli* (*E. coli*)) [44] or yeast (*i.e.*, *Pichia pastoris*) [45, 46] for amplification purposes in bioreactors and can also be expressed in mammalian cells for a therapeutic purpose. The major components involved within an engineered DNA plasmid are the origin of replication, promoter, GOI, and, in addition, commonly an antibiotic resistance gene for selection [47]. As for *E. coli*-based plasmid production, the composition of the culture media can vary from mineral-containing media to complex mixtures supplemented with yeast extracts. After replication in the bioreactor, bacteria can undergo a lysing process through alkaline or thermal treatments, followed by plasmid purification through precipitation/centrifugation [48, 49]. This large-scale pDNA production is cost-effective in comparison to LAV and IV manufacturing processes, possibly making the technology cheaper in the long run for consumers. The relatively recent development of minicircles (episomal DNA)/miniplasmids (*i.e.*, P1, P7, and F)/ministrings [50-55] can potentially be transported more easily through cellular barriers to improve bioavailability [51].

For the sake of brevity, a discussion of downstream processing was omitted. Please refer to the following articles for further downstream processing information: [56-58]

6. Safety and stability of DNA vaccines

To date, there is no licensed DNA vaccine for use in humans [59, 60]. The scientific community has high expectations for DNA vaccine use because of the following reasons: (1) the ability to control the transcribed and translated product, thereby controlling the ability of the antigen to not revert to a virulent pathogenic form; (2) the relatively low production cost of DNA vaccines; and (3) the innate stability of DNA vaccines for storage and transportation [61, 62] purposes.

Auto-immunity – A potential disadvantage of DNA vaccines is that they could potentially trigger autoimmune diseases by eliciting anti-DNA antibody production owing to the use of prokaryotic DNA vectors. Such vectors may contain unmethylated CpG sequences and may be recognized as a PAMP by the immune system (*i.e.*, TLR9) [13, 63] and can result in Th1-biased immune responses [64, 65]. In 1989, Gilkeson et al. [66] associated prokaryotic double-stranded DNA (dsDNA) immunization with the development of anti-dsDNA antibodies in mice. In 1994, Lilic et al. [67] described the induction of anti-DNA antibodies after the administration of a subunit vaccine against hepatitis B virus (HBV), and recently, Zafrir et al. [68] reported that the HBV vaccine induced an autoimmune syndrome when used with the required adjuvants. On the other hand, other studies suggested no direct effect of vaccinations triggering autoimmune diseases [69].

Insertional mutagenesis of viral and nonviral delivery methods – DNA vaccines may cause indel mutations, the risks of which depend on the mechanism of delivery. Despite nonviral gene delivery systems being safer than viral vectors, risks of insertional mutagenesis are not zero, although the risks are believed to be lower than those of everyday random mutations. Unfortunately, often such nonviral risks are based on the insertion of a

functional fluorescence-based marker where the entire functional sequence must be inserted not only within the genome but also into a region that is expressed. Nonviral risks of insertional mutagenesis may be higher than that currently believed. Such risks are also a function of the sequence and whether the DNA is supercoiled.

The administration of a DNA vaccine exposes the patient to foreign DNA or its fragments that could be inserted into the host's chromosomal DNA [70]. In the case of incorporation into an exon, an insertional mutation or a frameshift mutation occurs. Such mutations can cause a gene to malfunction or inactivate (*i.e.*, a tumor suppressor gene). The insertion of foreign genes into the host genome could also lead to constituent expression of previously silent bacterial/parasite genes that have been inserted. The insertion may also increase the probability of rearrangements or breaking. The guidelines for industrial production of DNA vaccines published by the FDA recommend that the pDNA is supercoiled to more than 80% to help prevent insertional mutagenesis. It has been reported that the FDA recommends integration studies, regardless of the delivery method, if there are greater than 10,000 copies of foreign DNA per microgram of host DNA [71]. Interestingly, minicircle DNA [51, 53, 54, 72, 73] and ministring DNA [74, 75] have been reported to have less risk of insertional mutagenesis because the major bacterial DNA (*i.e.*, the unmethylated CpG repeats functioning as PAMPs) is removed.

Environmental stability (nonbiological) – DNA vaccines have an advantage of not requiring such rigorous temperature control as the protein-based vaccines require. However, the stability of nucleic acid-based vaccines under dry conditions (*i.e.*, storage and transportation) or under aqueous conditions is highly dependent on stabilization techniques. Crine et al. [76] reported the stability of apurinic sequence sites to remain undamaged for approximately 288 to 335 h at 37°C, pH 7.21, and in a buffer solution that is similar to physiological media. Kami et al. [77] investigated the thermal degradation rates of pDNA (0.75 µg of pUC19) and found that there was complete degradation after 9 min at 170°C in an aqueous solution. When the pDNA was incubated at 200°C under aqueous conditions, no intact pDNA could be found after 20 s. In the case of dried pDNA, the degradation temperature was reported to have a low threshold. They incubated pDNA and pUC19 at 10°C increments for 5 min and found that pDNA started degrading at 130°C and completely degraded at approximately 190°C (in comparison to 95°C). In addition, of note, prokaryotic DNA was reported to be more thermally stable than eukaryotic DNA [78].

Biologically relevant stability – The stability of nucleic acids in the physiological environment depends on specific conditions at the intracellular, tissue, and systemic levels. In an *in vivo* environment, there is variation in pH (~5-7.45), exposure to various enzymes (*i.e.*, nucleases) and reactive oxygen species, as well as the possibility of being epigenetically modified or modified by host DNA repair mechanisms [79].

The development of delivery systems for nucleic acids (*e.g.*, polymeric and lipid vectors), which control the microenvironment of the nucleic acid, helps to maintain the molecular stability, as there is a decrease in the degradation rate when present in a complexed state (*i.e.*, polyplex and lipoplex) versus a free state [80]. For example, the *in vivo* half-life for a nonionically complexed DNA is approximately 10 min in the extracellular environment, whereas the intracellular half-life is long, close to 1-4 h. Despite the advantage in being in a complexed state in terms of its structural stability, if the DNA is excessively complexed, then successful transcription will not be as efficient, as the plasmid will not be accessible to the transcription machinery [81, 82].

Evans et al. [83] described the relevance of controlling the main mechanisms of DNA degradation (*e.g.*, depurination/β-elimination and free radical oxidation by employing chelators and hydroxyl radical scavengers). The use of ethanol and EDTA (ethylenediaminetetraacetic acid) or DTPA (diethylenetriaminepentaacetic acid) in DNA-based formulations is associated with enhancing the remaining DNA amount from approximately 30% to 70% after 1 month incubation at 50°C.

Peptide nucleic acids (PNAs) are uncharged molecules that demonstrate increased resistance against nucleases and RNases in comparison to endogenous nucleic acid, which can have benefits for specific gene delivery and DNA vaccine applications. The conjugation of PNAs with cell-penetrating peptides (CPPs) can enhance the molecular stability and facilitate transfection [84]. In addition to being highly stable, CPP-conjugated PNAs have improved DNA sequence recognition and a higher affinity with lipid membranes because of the peptide backbone [85].

Epigenetic modification affects the molecular stability and the genetic expression of DNA. Modifications such as DNA methylation are more likely to occur in CpG-rich regions [86], and the methylated regions may subsequently recruit DNA methylated-binding proteins and histone deacetylases (HDAC)s, which downregulate gene expression [87], as the transcriptional machinery cannot access the DNA.

7. Plasmid delivery

At a systemic level, eliciting specific antibody subtype responses depends on the contexts and routes of the delivery methods. For instance, the vaccine containing *Lactobacillus* vector against the influenza A virus induces a higher survival rate in a murine model when administered through the intranasal route than through the oral route [88]. IgA titers were measured for an anti-HIV DNA vaccine, and these titers were found to be increased for the intranasal route in comparison to the intramuscular (IM) route after DNA vaccination [89]. Vaccine administered through the IM route can induce greater IgG2a titers, whereas a gene gun method could elicit a greater IgG1 antibody response [90].

At a cellular level, the transportation of highly charged macromolecules such as DNA across a negatively charged phospholipid bilayer membrane and subsequently through the highly restrictive nuclear envelope is challenging. More specifically, the main barriers for the delivery of pDNA vaccine are as follows: stability (described in the previous section), cellular uptake, endolysosomal escape, decomplexation from the carrier, and nuclear envelope translocation. The cellular uptake of nonviral gene delivery carriers can be taken up through clathrin-, caveolae-mediated endocytosis, or macropinocytosis (endocytic pathways) [91, 92]. Plasmids can be internalized within the nucleus through intranuclear injection, direct/indirect nuclear localization signals (i.e., DNA-targeted sequences), and encapsulation by the nuclear envelope upon reformation postmitosis [93].

7.1. Physical methods for DNA vaccine delivery

Electroporation – Electroporation (EP) causes transient pores in the plasma membrane of host cells to increase the uptake kinetics of pDNA under an electrical field. In a recent clinical trial, a DNA vaccine was delivered by IM-EP using Ichor Medical Systems TriGrid™ Delivery system (TDS-IM) [94]. The results demonstrated that the DNA vaccines delivered by EP are safe and effective for eliciting strong immune responses.

Gene gun – Another physical method developed to deliver plasmids epidermally is THE gene gun [95]. A particle-mediated epidermal delivery (PMED) gene gun was used in preclinical trials to deliver a DNA vaccine against the dengue virus in nonhuman primates. Plasmids including the oligonucleotide sequence of vaccine antigens were precipitated onto 1 µm-diameter gold beads. The DNA-adsorbed gold beads were then delivered using a gas-pressurized gene gun, which is a needle-free device [96]. The difference in PMED in terms of IM and intradermal injections using a needle and syringe is that PMED enables direct delivery of the vaccine into the intracellular environment more efficiently, thereby improving the cellular uptake and resulting in higher immune responses with substantially lower doses (100- to 1000-fold) of DNA [97]. Choi et al. [98] compared three different delivery methods (IM, intradermal, and epidermal inoculation) using plasmid-coated gold beads through particle-pressurized bombardment (i.e., gene gun). The intradermal injection and gene gun resulted in specific IgG antibody responses but not IgA. Despite the induction of IgG responses, both the gene gun and intradermal administration methods failed to protect mice from a rotavirus infection in that study.

Other physical methods have included physically puncturing the cells by using microneedles (impalefection) [99], hydrostatic pressure, squeezing cells in a microfluidic chamber (in addition to EP) [100], sonoporation [101], and intranasal delivery [38]. For interested readers regarding physical methods for intracellular delivery, we would recommend the publications from Meacham et al [102, 103].

Pros: EP and gene gun are safe to use for delivering DNA and have shown immune responses in specific applications. EP requires less DNA without compromising efficacy. Cons: EP is often invasive and limited for in vivo applications and may lead to cell death. The gene gun method has limited or no control over the insertion sites of the DNA and is relatively expensive [104].

7.2. Nonviral methods (lipid and polymer based)

Lipid or cationic, amine-containing polymers are often complexed with anionic plasmid macromolecules into nanosized particles, and this facilitates cellular uptake and inhibits the degradation of the plasmid during trafficking both extracellularly and intracellularly. In an uncomplexed state, half-lives of plasmids extracellularly in serum and intracellularly is in the order of a few minutes and hours, respectively. The mass of free polymer carrier in the solution is critical for the delivery efficiency and is typically administered in many fold excess for transfection to occur. Owing to the need for free polymer to be in excess, despite taking advantage of the enhanced permeability and retention effect for the larger polyplexes, the free polymer is not able to sufficiently transport to the site of interest [105]. For this reason, nonviral gene delivery systems are often injected

locally. Furthermore, many researchers have endeavored to improve the buffering capacity, but generally, the carriers are excessively toxic by doing so. Interested readers may refer to the following review for further information with regard to nonviral gene delivery barriers [106-108]. The following paragraphs discuss cell specificity, hydrophobicity, the proton sponge effect, and nuclear uptake for the readers' convenience.

Cell specificity of nonviral gene delivery systems – With regard to the cell specificity, surface modifications can be employed for enhancement of uptake and structures of the carriers can be screened by using high-throughput methods to discover cell specificity [109]. Guerrero-Cázares et al. [110] demonstrated that biodegradable poly(beta-amino ester) nanoparticles present specific transfection efficacy to human brain tumor-initiating cells compared to noncancerous cells. Similar results were also reported in a previous work on hepatoma cells [111] and glioblastoma cells [112]. The exact mechanisms of material structure-related cell specificity remain unknown. However, it is important to note that the cell specificity of the nonviral gene delivery system was not due to factors such as cellular division rate, cellular uptake amounts of nanoparticles, or media composition. Although the exact mechanism remains exclusive, it is hypothesized that different pathways of endocytosis tuned by different polymer structures may be the answer to cell specificity. Understanding the Structure Activity Relationships (SARs) is an ongoing endeavor within the field. Enabling the ability to engineer optimized delivery systems is the objective in elucidating such SARs.

Hydrophobicity of nonviral gene delivery systems – An analysis of the interaction of the cell membrane with amphiphilic materials has demonstrated that adsorption of hydrophobic moieties (i.e., Lipofectamine2000®/3000®, lipid-based or a greater number of carbons in the polymer backbone or side chain) can cause disruption or destabilization of the cell membrane, thereby facilitating endosomal uptake [81, 113, 114]. Therefore, promoting cellular uptake is often accomplished by using polymers or lipids designed to increase the interaction between nanoparticles and the cell membrane.[82] Hydrophobicity is one of the main variables that is varied to optimize a nonviral gene delivery system.

Proton sponge effect for nonviral gene delivery systems – After internalization through an endocytic pathway, the pDNA needs to efficiently escape from the endolysosomal degradation pathway into the cytoplasm to avoid degradation. Several authors have described a greater endosomal escape using polyethyleneimine (PEI) conjugated to the pDNA to further enhance the “proton sponge effect,” which promotes endosomal swelling and rupture [115]. This effect occurs because of the buffering capacity of the unprotonated amine groups on PEI, thereby creating an imbalance in charge and osmotic pressures across the membrane. Thus, there is an influx of Cl⁻ ions and water molecules into the endosome [116]. Other escape mechanisms have involved fusogenic peptides. For example, Nakase and Futaki suggested the association between PEI and the fusogenic peptide GALA on the cationic lipid-coated exosomes, which increased endosomal escape of exosomes that are useful for nucleic acid delivery. Hu et al. [117, 118] developed a DNA vaccine against malignant melanomas employing TAT-based fusogenic peptides with PEI-mannose nanoparticles adsorbed onto microneedles. The use of the TAT-based fusogenic peptide resulted in T-cell activation and enhanced expression of IFN γ IL-12 [119].

Nuclear uptake – A nuclear localization sequence can also be indirectly incorporated into the pDNA by using DNA targeting sequences (DTSs) [120]. A DTS is a DNA subsequence that can be incorporated into the pDNA and is a binding site for NLS-containing protein. Presumably, after the DNA is separated from the complex, karyopherins are able to help facilitate the nuclear uptake of the plasmid. This technology was derived from viruses, for example, the simian virus 40 (SV40), which has a DTS within its genome [80, 121], uses this mechanism to improve its ability to replicate. Thus, when the following SV40 sequence (5'-AACCAGCTGTGGAATGTGTGTCAGTTAGGGTGTGGAAAGTCCCCAGGCTCCCCAGCAGGCAGAAGTATGCAAAGCAT-3') is incorporated into the pDNA of interest, improved gene transfection can similarly be observed [122].

Pros: Nonviral delivery systems are relatively safer to use than their viral counterparts and benefit from being more cost-effective and easier to chemically modify and optimize. Cons: Nonviral systems generally result in temporary expression and also relatively lower expression during the period of expression [123].

8. Controlling gene expression through plasmid engineering and gene circuits

Designing a plasmid entails the selection of the DNA insert or the GOI, the DNA vector or backbone of the plasmid, the transformation protocol depending on the species of the host organism (i.e., competent cells are often used for transformation in *E. coli*), and the host organism (i.e., bacteria (*E. coli*) or yeast (*P. pastoris*)).

Minicircle DNA and CpG repeats – Relatively recent technologies suggest that the use of minicircle DNA increases therapy biosafety because bacterial DNA is removed from the parental plasmid such that only the GOI and promoter/terminator sequences remain [124]. Because parental bacterial sequences are absent to a greater extent, the lack of CpG sequences has resulted in long half-lives of the plasmid. However, for specific applications, encoding CpG is desirable for enhancing the immunogenic response. Moreover, studies have demonstrated that gene transfer using minicircles induces a 10- to 1000-fold increase in the long-term transgene expression *in vivo* and *in vitro* when compared to pDNA for specific applications, which can potentially improve the immunogenicity of DNA vaccines [125].

To improve pDNA TGE efficiency, early studies investigated various combinations of promoters/enhancers to control gene expression, as well as the TGE efficiency for HIV-1 vaccination [126, 127]. Sun et al. [128] and Li et al. [129] reported the use of post-translational regulatory elements to improve the efficiency of DNA vaccines. Such approaches will likely benefit the field.

Codon optimization – Codon optimization adapts DNA sequences between species to augment expression. Amino acids are coded by synonymous genetic codons, and the frequency of the synonymous codon being used depends on the species. Gene expression can be optimized by utilizing the advantage of information of codon usage in specific organisms. During the plasmid design, low-frequency eukaryotic codons in the foreign DNA backbone are identified and replaced for high-frequency codons, however, maintaining their respective coded amino acids [130-132]. There has been recent progress in terms of enhancing the immunogenicity in mice and chicken primed with such codon-optimized DNA vaccines [133-135].

Synthetic biology – Synthetic gene circuits provide tools for accurately controlling gene expression [136]. The plasmid sequence itself can be engineered to control the expression [137, 138]. For example, gene circuits in conjunction with CRISPR technology where two single-nucleotide polymorphisms related to the occurrence of colon cancer are detected and the cas9 enzyme is used to control the expression of target genes [139]. Brophy and Voigt [140] constructed a gene circuit in *E. coli* with an antisense promoter placed next to the terminator to study the function of antisense promoters as a regulator. The same group has also worked on designing computation tools such as the python language-based “DNAplotlib” library to visualize the gene circuit outline [141]. Another application using gene circuits and synthetic biology is the orthogonal polymerases, which independently control multiple pathways in the same cell [142]. Using multiple activator-chaperone pairs has also been observed to improve the orthogonality in gene circuits [143]. Moon et al. [143] used a four-input AND gate that controlled the orthogonal gene expression of multiple pathways at the same time, independent of each other employing *E. coli*.

Deans et al. investigated a mechanism that enables control over the gene expression profile through engineered inducers within genetic circuits [136], thus demonstrating the potential to switch a GOI on/off through molecular controllers. Such applications could potentially enable the regulation of the immune response in terms of intensity and type (cell mediated/humoral) in the future for vaccine applications. Recently, synthetic biology has been widely used for genetic engineering applications to conduct developmental and functional studies.

Pros: Plasmid engineering is a potential method to control gene expression, but currently, technology is generally limited to nontherapeutic genes. As this nascent field continues to grow, there will likely be great improvement in terms of controlling expression as a function of the presence or absence of key entities. Synthetic biology in particular provides a number of tools such as CRISPR to efficiently add or delete the GOI and improve specificity and off-target effects. Cons: Extraneous mutations (i.e., indels) can often occur in technologies as CRISPR, thereby leading to severe side effects. The complexity of certain gene circuits can lead to unreliable gene expression and safety concerns that will need to be thoroughly investigated.

9. Techniques to overcome immunogenic issues of DNA vaccines

Despite the positive outlook, DNA vaccines have low immunogenicity and hence require immunostimulant adjuvants and/or additional priming or booster. The immunostimulants and adjuvants, depending on the type, may, however, require more complex storage and transportation conditions. Methods involving the use of cytokines (i.e., IL-4) or the granulocyte-macrophage colony-stimulating factor (GM-CSF) have proven useful in enhancing the immune response. For example, Kalams et al. [144] reported that IL-12 and/or IL-15 produced a safe and immunogenic HIV-1 *Gag* DNA vaccine. Kalams et al. also evaluated the positive impact of EP delivery methods for the HIV-1 *Gag* antigen/IL-12 adjuvant plasmid vector in a phase I clinical trial. Other studies have also assessed the immunogenicity of DNA vaccines containing chemokine-expressing

sequences for HIV-1 immunization [144-146]. CpG oligonucleotide (ODN) is another common genetic adjuvant used for DNA vaccines [9, 147, 148]. Preclinical studies have demonstrated that CpG ODN activates TLR9-bearing B cells and plasmacytoid dendritic cells and further support the induction of strong Th1-type response [149]. In addition to engineering the ratio of CpG motifs in DNA vaccine to improve immunogenicity, administering additional synthetic CpG ODNs or co-administering a second plasmid cloned with CpG motifs has been investigated. Kojima et al. delivered a CpG-encoding plasmid 2 days and 4 days both before and after an HIV DNA vaccine was delivered (as well as at the same time). Results showed that a significant boost of HIV-specific IgG and cytotoxic T lymphocyte activity can be obtained when the CpG plasmid was administered either 2 or 4 days after HIV DNA vaccination [150].

Consecutive immunization by using a prime/boost strategy is also applied in many clinical trials to overcome poor immunogenicity of DNA vaccines. The immunization involves priming by a DNA vaccine followed by boosting with recombinant protein vaccine encoding common antigens [151]. For example, pDNA vaccines and recombinant fowlpox virus (rFPV) vaccines are investigated to be potential candidates of HIV-1 vaccine. Dale et al. demonstrated this prime-boost vaccine can induce stronger antigen-specific T-cell response [152]. A large and immediate T-cell immune response was observed after administering rFPV boost in macaques 12 days after priming with DNA vaccines. However, a similar boost in immunity may not be obtained while reboosting with a second dose of the same recombinant protein vaccine. This suggests that the doses and the intervals between doses for multiple boosting vaccinations need to be further evaluated to stimulate continuous T cell immunity.

10. Examples of DNA vaccine commercial successes

According to the DNA vaccine database DNAVaxDB [153], there have been more than 20,000 articles related to DNA vaccine up to and including the year 2017 indexed in PubMed and Google Scholar. However, to the extent of our knowledge, there has not yet been a licensed DNA vaccine for use in humans in the U.S., Europe, or Japan. Because the gene-based formulation requires greater safety evaluation than conventional vaccines (*e.g.*, nucleic acid integration into the host's chromosomal genome), the timeline for approving DNA vaccines for humans is relatively lengthy. While many human DNA vaccines are still being evaluated in clinical trials, to the extent of our knowledge, there have been four DNA vaccines approved for veterinary applications. Overviews of DNA vaccines approved for animal models have been reported in several articles [154-156]. These approved DNA vaccines are for a number of species including equine, salmon, porcine, and canine. The earliest DNA vaccine approvals were obtained in 2005, namely, West Nile–Innovator® (equine) and Apex-IHN® (salmon). These two vaccines are prophylactic vaccines for infectious diseases encoding subcomponents of the viral proteins for generating antibodies against the West Nile Virus and the infectious hematopoietic necrosis virus, respectively. In 2008, a single dose of vaccine expressing the growth hormone Life Tide® SW5 (*i.e.*, porcine) was licensed for gene therapy. The latest approval was in 2010, namely, Oncept™ (canine), which is used for cancer immunotherapy against oral melanoma (**Table 3**). Although the noninfectious vaccines are not the main focus of this review, the two vaccines are included in **Table 3** to provide a whole picture of the current progress on DNA animal vaccines.

To date, there are a number of clinical interventional trials in the U.S. and in 201 other countries evaluating human DNA vaccines, according to the a search with “Vector vaccine” (71), “DNA vaccine” (169), “plasmid vaccine” (79), on ClinicalTrial.gov [157]. Studies with unknown status/withdrawn are excluded from these numbers. Details on patented and/or sponsored DNA vaccine technologies are summarized in **Table 4**. The majority of these trials (13 of 18 selected trials) are investigating prophylactic vaccines for infectious diseases (*i.e.*, HIV, influenza, and hepatitis B infections). A detailed analysis of clinical trials of gene-based prophylactic vaccines (including virus vaccine) was reported by Nakayama et al. in 2015 [158].

To date, most clinical trials have demonstrated no significant evidence indicating DNA insertional mutagenesis into the chromosomes of hosts and immunologic tolerance in terms of developing anti-DNA antibodies. However, the transfection efficiency of DNA plasmids is generally poor resulting in an insufficient induction of an immune response, which is possibly one of the greatest challenges in current clinical trials. As a result, more trials have been utilizing hybridized formulations (*i.e.*, CpG) and/or higher DNA doses for greater immunogenicity [151]. Current clinical trials for HIV infection are an example of such endeavor. The GOVX-B11 vaccine, currently in phase II trial, constitutes two components: a DNA vaccine used to prime a person's immune response and a recombinant MVA (modified vaccinia Ankara, attenuated vaccine) used to boost the primed

response. Their studies were conducted in HIV-infected participants who currently undergo antiretroviral treatment. It has been demonstrated that GOVX-B11 is capable of eliciting antibodies and a T cell response against a heterologous challenge [159]. On the other hand, the PENNVAX DNA vaccines developed by Inovio Pharmaceuticals, currently in phase I clinical trial, utilize the prime-boost strategy same as that of GOVX-B11 by combining a viral vector vaccine. Further, Inovio demonstrated that the immune response can be enhanced when delivered by *in vivo* intradermal EP of PENNVAX compared to a syringe injection [160, 161]. These results reveal that the modification of DNA vaccine formulations or combinatorial delivery approaches can improve the potency and efficacy of DNA vaccines in human clinical trials.

In summary, as of 2017, a large number of second-generation vaccines have been licensed and released on the market. Some of these DNA vaccines have also been approved for sale in animal health (summarized in **Tables 2 and 3**). These reports provide evidence for the potential and growth of a market for new vaccine technologies. Regarding the feasibility of current trials of DNA vaccines, further advancement of the plasmid formulation and delivery approaches will be the necessary for the continued improvement of the potential DNA platform.

11. Conclusion and Future Directions

The optimization of vaccine scheduling has been generally limited to investigations where time was varied by month [162]. Optimizing vaccine schedules to smaller steps in time will likely result in enhanced seroconversion and protection. In terms of engineering the kinetics for vaccines by auto-boosting technologies, the practicality of receiving doses on short time scales is increasingly more reasonable. New technologies such as SEAL [163] are seriously needed and are likely to be highly impactful. Potential complications such as the junction of the seal must be mitigated to the extent possible. Removal of the need to seal would be advantageous but highly challenging. Such endeavors would be likely worthwhile.

Enhancing the ability to stabilize the cargo within is challenging. Having a depot environment that is optimized and catered to a given antigen is possible within a depot vaccine system in terms of excipients and cryoprotectant content, as well as ratios of excipients to antigen. However, if multiple antigen types are to be delivered from the vaccine depot, it is highly challenging to cater to multiple antigen types in the most optimal fashion within a single depot. Endeavors to deliver vaccine depots with environments that are most optimally catered to each specific antigen within a given injectable vaccine system would also be beneficial and challenging from an engineering standpoint.

To date, although clinical translation of gene-based systems has been limited, the U.S. has recently approved two gene therapies. As more gene-modulating technologies receive approval, obtaining 510(k) clearance will be increasingly common for this field. DNA vaccines, although promising, suffer limitations owing to their inability to be sufficiently immunogenic. Techniques to engineer DNA-based systems such as prime/booster methods, as well as the incorporation of adjuvants (transcribed/translated or codelivered), will continue to improve the immunogenicity for attaining protective seroconversion.

Currently, safety assessments for gene delivery systems undergoing approval processes are arduous to determine risks of insertional mutagenesis. Although gene sequencing is becoming increasingly cheaper over the years, conducting qRT-PCR or qPCR is time consuming and requires relatively more sophisticated instrumentation in comparison to fluorescence-based assays. Endeavoring to properly assess insertional mutagenesis risks for gene-modulating technologies would probably be highly useful if the assay is fluorescence based and sufficiently reliable.

To further the development of vaccines with improved functionality, an interdisciplinary-focused research will be of great utility. In light of research discussed herein, the vaccine realm will be experiencing great improvements in the following areas in the coming years: further optimization of vaccine scheduling; duration of protection through nonkinetic approaches; enhancement of antigen stability; improved immunogenicity of DNA vaccines; manufacturing and engineering vaccines in general, and the ability to control gene circuits for gene-modulating technologies.

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Table and Figure Captions

Table 1. Generalized qualitative comparisons of vaccine classifications. Please note that a few exceptions may contradict the generalized qualitative comparisons. Details on administration routes, advantages and disadvantages regarding production, immunogenicity, biosafety, transportation/storage, and examples of commercialized DNA- and amino acid-based vaccines for each vaccine classification are tabulated.

Table 2. Examples of adjuvants [19-22, 144-146, 164-198].

Table 3. Recent licensed protein and DNA vaccine therapies (data extracted from 2001 to 2017, some of which are not related to infectious diseases).

Table 4. Selected current DNA vaccines in the progress of Phase I to III clinical trials.

Fig. 1. Research trends of various vaccine types. Values are based on PubMed results (which could be an indicator for popularity) using EndNote between 1931 and 2020, where the projected values, as indicated by an asterisk (*) for 2011-2020, were calculated by multiplying the current values by the ratio 120/87.5. The total number of months is 120, and the number of months to date within the time period of interest (Jan 2011 to April 2018 (87.5)) is 87.5. The following keywords were entered into the “title” form in EndNote when searching for PubMed research

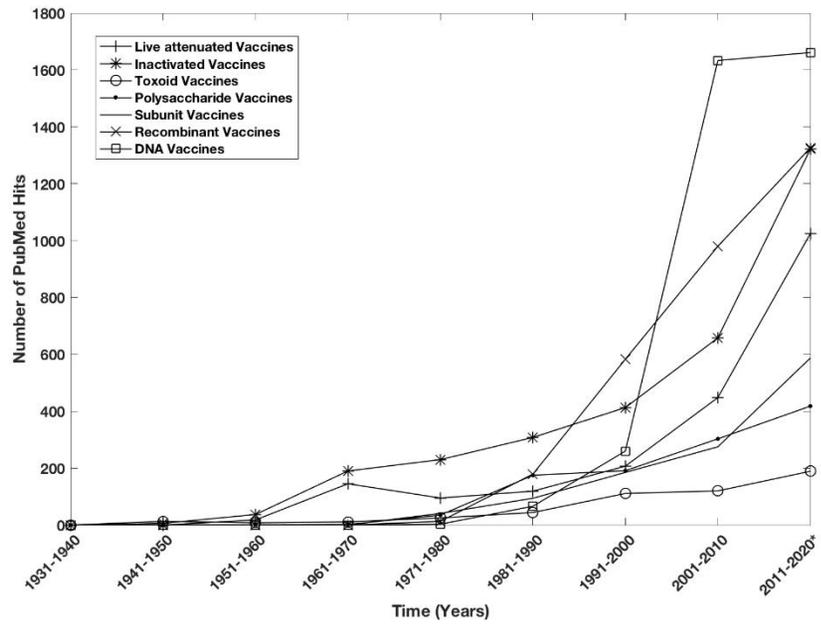
articles: subunit vaccine, live attenuated vaccine, toxoid vaccine, inactivated vaccine, polysaccharide vaccine, recombinant vaccine, and DNA vaccine. The total number of results would be different, however, if the abstract or other keywords had been queried.

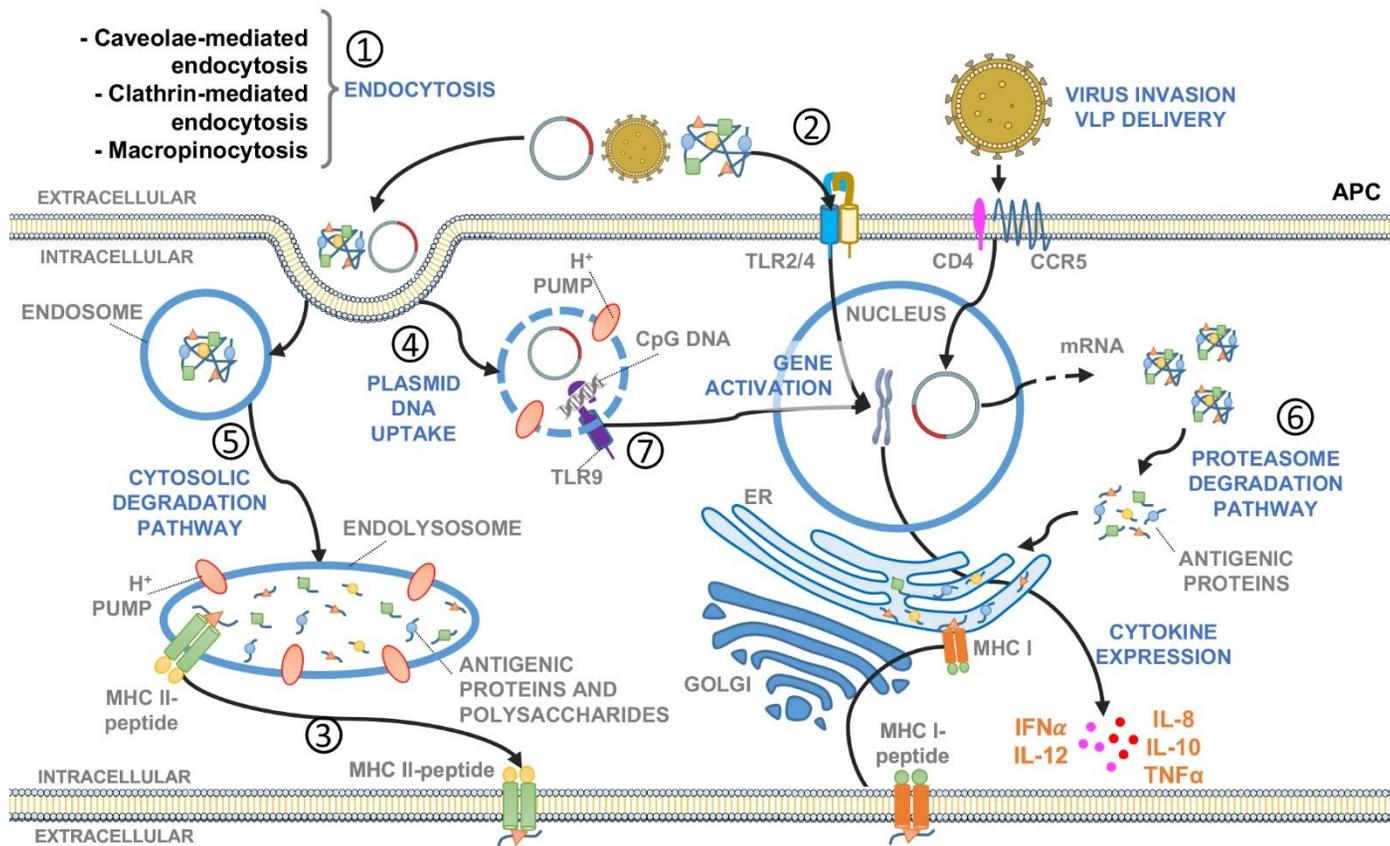
Fig. 2. DNA- and amino acid-based antigen internalization and processing. (1) endocytosis; (2) extracellular activation through TLR2/4 resulting in the expression of proinflammatory cytokines and chemokines (IL-8/10, TNF α); (3) Proton sponge effect for DNA vaccines (4) CspG sequences activating TLR9 and resulting in IL-4 and IFN α release; (5) cytosolic degradation pathway resulting in (6) MHC II antigen presentation to CD4⁺ T cells; (7) proteasome degradation pathway and the eventual MHC I antigen presentation to CD8⁺ T cells. Direct somatic cell engulfment/antigen-presenting cell (APC) display entails (1, 5, 3), leading to MHC II-peptide display. Steps for phagocytosis of a transfected (nonviral) or transformed (viral) cell/cross-priming entails (1, 4, 6), leading to MHC I-peptide display. Steps for Toll-like receptor (TLR) activation entails (2, 7).

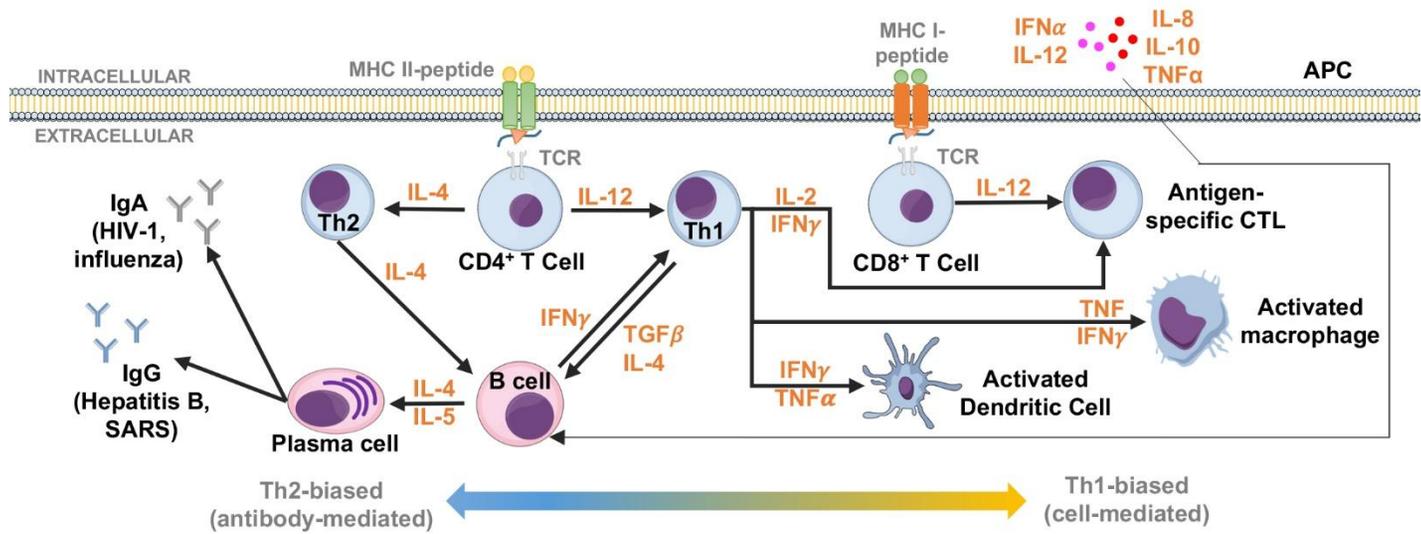
Fig. 3. DNA- and amino acid-based antigen presentation. Th2-biased (antibody-mediated) and Th1-biased (cell mediated) responses, depending on the context of antigen presentation.[199] (APC, antigen-presenting cell; CCR5, C-C chemokine receptor type 5; CpG DNA, DNA fragment containing cytosine nucleotide followed by guanine nucleotide; CTL, cytotoxic T lymphocyte; ER, endoplasmic reticulum; IFN, interferon; Ig, immunoglobulin; IL, interleukin; MHC, major histocompatibility complex; TCR, T cell receptor; Th, T helper cell; TNF, tumor necrosis factor; TRL, Toll-like receptor; VLP, virus-like particle).

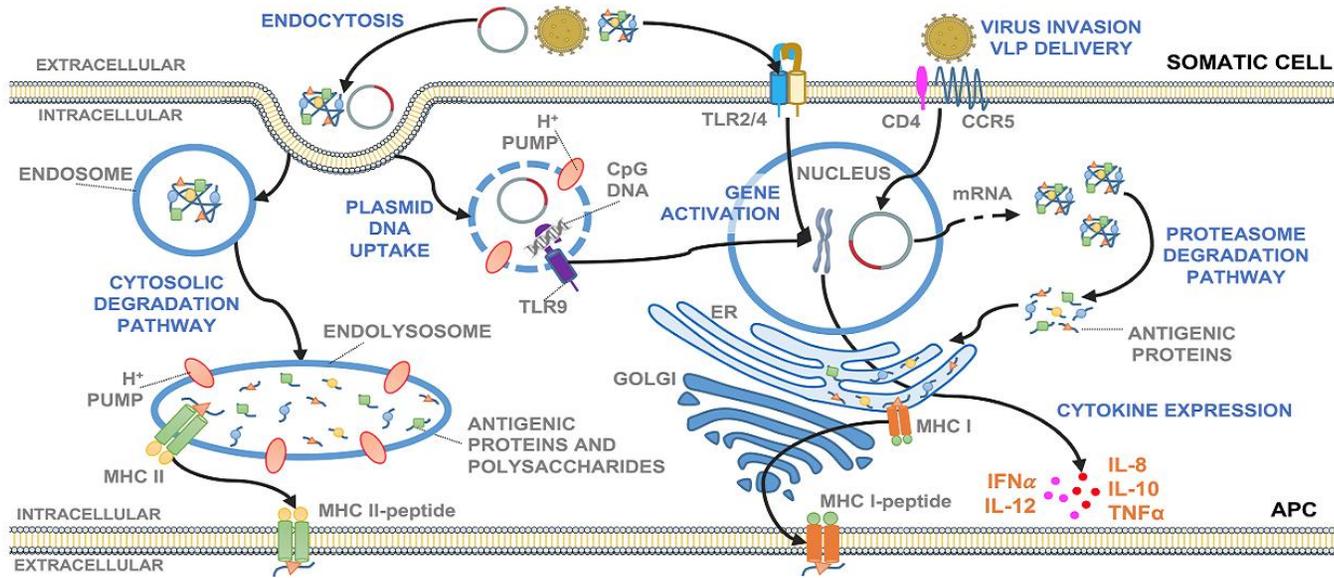
Fig. 4. Polymer-based delivery system 1. (A) Silk/PAA composite microneedle micrograph (scale bar: 500 μ m); (B) OVA release from silk/PAA microneedles measured by fluorescence; (C) microfabricated PLGA microparticle before antigen dispensing (left, scale bar: 100 μ m) and after thermal sealing (right, scale bar: 500 μ m); (D) antigen release in pulsatile kinetics measured by fluorescence; (E) antigen distribution in PLGA microspheres submitted for short (left) and long solvent evaporation time (right, scale bar: 20 μ m); (F) different antigen release profiles obtained for short and long solvent evaporation time.

Fig. 5. Polymer-based delivery system 2. (A) IPV antigen-containing PLGA microspheres with 7.5% EPO (left) and 5% EPO/0.4% L-arginine (right, scale bar: 20 μ m); (B) IPV antigen release profile changes drastically with the microparticle composition; (C) micrograph of the wirelessly controlled implantable PLGA microchip before (left) and after (right, scale bar: 50 μ m) triggering the antigen release; (D) antigen release rate shows a well-defined pulsatile release. Adapted with permission from Ref. [200-204].









	Live attenuated vaccines	Killed or Inactivated vaccines	Inactivated toxoid vaccines	Polysaccharide vaccines	Conjugate polysaccharide vaccines	Recombinant protein vaccines	DNA vaccines
Further Classification	Whole-cell vaccines	Whole-cell vaccines	-	Subunit vaccines	Subunit vaccines	Subunit vaccines	Subunit vaccines
Administration	<i>i.e.</i> , subcutaneous, percutaneous, oral, intranasal	<i>i.e.</i> , intramuscular, intradermal, subcutaneous	<i>i.e.</i> , intramuscular	<i>i.e.</i> , intramuscular, subcutaneous		<i>i.e.</i> , intramuscular	<i>i.e.</i> , intramuscular Mucosal
Production	- Bacteria applications + Virus culture + Large-scale production - Biocontainment	+ Low-cost production + Large-scale production	- Toxin purification procedures - High-cost production	+ Bacterial capsule components - Biocontainment		- Protein folding - Protein degradation + Encapsulation	+ Molecular stability + Low-cost production + Encapsulation
Immunogenicity	+ Natural infection + Immunization efficiency + Single or few doses + Life-long protection	+ Natural infection - Multiple doses - Adjuvant use + Long-term protection	- Multiple doses - Adjuvant use	+ Molecular pathogen - Multiple doses - Adjuvant use	+ Stimulus by Conjugation - Multiple doses - Adjuvant use	+ Particle design - Multiple doses - Adjuvant use	+ Animal applications - Human applications + Particle design
Biosafety	- Risk of infection - Risk of reversion - Risk for the immuno-incompetent	+ Safer than LAVs	+ Fewer side effects (<i>i.e.</i> , local and systemic)	+ No live pathogenic components + Fewer side effects			+ No live components + Fewer side effects - Autoimmune response - Integration to genome - Indel mutations
Storage and Transportation	- Cold chain delivery	- Cold chain delivery	+ No need for cold chain delivery	+ No need for cold chain delivery	+ No need for cold chain delivery	+ No need for cold chain delivery	+ No need for cold chain delivery
Licensed vaccines (trade names)	M-M-R II, OPV, FluMist, Rotarix, ProQuad, Adenovirus, Zostavax	Pediarix, Ipol, BioThrax, Infanrix, Daptacel, Gardasil, Cervarix, Flublok	Decavac, Tenivac	Menomune, Pneumovax 23	PedvaxHIB, Hiberix, Comvax, Pevnar 13	Engerix-B, Rcombivax HB	-

Adjuvant	Composition	Disease	Vaccine Type (commercial name)	Immune response	Research stage	Year
Alum	Alum, 3-O-desacyl-4'-monophosphoryl lipid A (AS04®) (GSK MPL®)	Influenza A	Virus-like particle (M2eVLP)	improved cross-protection	mice	2014
		Human Papillomavirus	Protein vaccine (HPV-16 L1/HPV-18 L1) [GSK Cervarix®]	enhanced antibody response	clinical study (girls 9-14 years)	2015
		Toxoplasmosis	DNA vaccine (toxifilin gene)	enhanced humoral response and switched from Th2 to Th1	mice	2016
		Hepatitis B	Protein vaccine (HBsAg) [GSK FENDrix®]	enhanced humoral and cell-mediated immune responses	clinical study (renal-transplanted patients)	2017
Squalene oil-in-water emulsions	Squalene, montane 80, eumugin B1 PH (AF03®) Squalene, MPL®, saponin (QS21®) (AS02®) Squalene, tween 80, sorbitan triolate (MF59®)	Influenza	Protein vaccine (haemagglutinin)	enhanced humoral immune response	mice	2014
		Pneumonia	Protein vaccine (PhtD)	increased frequency of CD4 ⁺ T cells and memory B cells	Phase I	2015
		HIV-1C	Protein vaccine (gp140)	enhanced humoral and cell-mediated immune responses	Phase I	2016
		Influenza A/H5	Protein vaccine (rHA) [Panblock®]	met criterion for seroconversion rate	Phase II	2017
Liposomes	Squalene, tween 80, α -tocopherol (AS03®) MPL®, saponin (QS21®) (AS01®) DDA®, TDB® (CAF01®)	Influenza A/H5N1	Inactivated virus vaccine (SV)	increased levels of IL-6 and IP-10 within 24 hours after vaccination	Phase I	2017
		Malaria	Protein vaccine (RTS,S) [Mosquirix®]	immunoprotection for 3-4 year infants, enhanced efficiency with booster	Phase III	2015
		Varicella-zoster virus	Subunit vaccine (HZ/su) [GSK Shingrix®]	significant immune protection in adults \geq 50 years	Phase III	2015
		Tuberculosis	Subunit vaccine (H56/CAF01®)	longlasting immunoprotection and enhanced CD4 ⁺ T cell response	Phase I	2016
TLR ligand	GLA-AF (TRL4 ligand) dsRNA analog Poly(I:C) (TRL3 ligand) CpG 1018 (TLR9 ligand) (Dynavax HEPLISAV-B®) CpG 7909 (TLR9 ligand) Cationic antimicrobial polypeptide/IC31® (TLR9 ligand) Alum-adsorbed GLA/SLA (TRL4 ligand) Lipopolypeptide Pam2/Pam3 (TLR2/6, TLR2/1 ligand) dsRNA analog Poly(I:C) (TRL3 ligand) Alum-adsorbed GLA/SLA (TRL4 ligand) Alum-adsorbed SMIP7.10 (TRL7 ligand) Imidazoquinolines (TLR7/TLR8 ligand)	HIV clade C	DNA vaccine/Attenuated vaccine/Protein vaccine (HIV env/gag-pol-nef, MVA-C, HIV CNS4dp140)	enhanced T and B cell immune responses	mice	2014
		Seasonal influenza	Inactivated vaccine (TIV)	enhanced humoral response	mice	2014
		Human Papillomavirus	Subunit vaccine (HIV-1 gp140)	longlasting IgG/IgA response	mice	2016
		Hepatitis B	Protein vaccine (HBsAg) [Dynavax HEPLISAV-B®]	enhanced superior seroprotection	Phase III	2015
		Meningococcal infection	Subunit vaccine (dLPS/OMP)	early and increased IgG/IgM response	Phase I	2015
		Tuberculosis	Protein vaccine (H4:IC31®)	high frequency CD4 ⁺ T cells and longlasting memory response	Phase I	2015
		Malaria	Protein vaccine (GMZ2.6C)	enhanced parasite-specific antibody and induced Th1 response	mice	2016
		Parasitic helminths	Autoclaved vaccine (ALM+Pam2/Pam3)	Th2 polarization	mice, parasite	2016
		Cancer	Protein vaccine (Db126 WT-1)	infiltration of CD8 ⁺ T cells in tumor	mice	2016
		Human Papillomavirus	Subunit vaccine (HIV-1 gp140/HSV-2 gD)	longlasting IgG/IgA response	mice	2016
Polysaccharide	Alum-adsorbed GLA/SLA (TRL4 ligand) Alum-adsorbed SMIP7.10 (TRL7 ligand) Imidazoquinolines (TLR7/TLR8 ligand) Inulin (Advax®) Chitosan	Malaria	Protein vaccine (GMZ2.6C)	enhanced parasite-specific antibody and induced Th1 response	mice	2016
		Meningococcal infection	Conjugated polysaccharide vaccine (MenC-CRM197)	Th1 polarization	mice	2016
		various	various	Th1 polarization	clinical study (newborn)	2016
		Hepatitis B	Protein vaccine (HBsAg)	enhanced humoral and cell-mediated immune responses	Phase I	2014
Genetic Adjuvant	PPE44/pCI-OVA CTA C-terminal HSP70 GM-CDF	Seasonal influenza	Inactivated vaccine (TIV)	low-dose TIV/Advax® induced efficient immune response	Phase I	2016
		Tetanus	Toxoid vaccine (TT)	enhanced mucosal immune response	-	2014
		Influenza	Subunit vaccine (HA-split)	enhanced humoral and cell-mediated immune responses	-	2014
		various	various	Th1 polarization	-	2015
Genetic Adjuvant	IL-12/IL-15 plasmid IL-12 plasmid NF- κ B subunit p65/RelA, Type-1 transactivator T-bet PPE44/pCI-OVA CTA C-terminal HSP70 GM-CDF	Hepatitis B	Protein vaccine (HBsAg)	enhanced humoral and cell-mediated immune responses	Phase I	2014
		Seasonal influenza	Inactivated vaccine (TIV)	low-dose TIV/Advax® induced efficient immune response	Phase I	2016
		Tetanus	Toxoid vaccine (TT)	enhanced mucosal immune response	-	2014
		Influenza	Subunit vaccine (HA-split)	enhanced humoral and cell-mediated immune responses	-	2014
		various	various	Th1 polarization	-	2015
		various	various	Th1 polarization	clinical study (newborn)	2016
Genetic Adjuvant	IL-12/IL-15 plasmid IL-12 plasmid NF- κ B subunit p65/RelA, Type-1 transactivator T-bet PPE44/pCI-OVA CTA C-terminal HSP70 GM-CDF	Tuberculosis	Live attenuated vaccine/pDNA (BCG)	enhanced T and B cell immune responses	mice	2014
		Cholera	DNA vaccine (HIV-1 Tat-Rev-Vif-Integrase-Nef)	upregulation of IL-6, IL-1 β	mice	2014
		Infectious bursal disease (chicken)	DNA vaccine (VP2 gene of IBDV)	enhanced humoral and cell-mediated immune responses	chicken	2015
		Cancer	DNA vaccine (MUC1-VEGFR2)	inhibition of tumorigenic cell growth	mice	2016
		Influenza	DNA vaccine	no enhanced immune response, tolerable adjuvanted-vaccine	Phase I	2012
		HIV-1	DNA vaccine	induction of CD4 ⁺ /CD8 ⁺ T cell response	Phase I	2013
Genetic Adjuvant	IL-12/IL-15 plasmid IL-12 plasmid NF- κ B subunit p65/RelA, Type-1 transactivator T-bet PPE44/pCI-OVA CTA C-terminal HSP70 GM-CDF	Hepatitis B	Protein vaccine (HBsAg)	enhanced humoral and cell-mediated immune responses	Phase I	2014
		Seasonal influenza	Inactivated vaccine (TIV)	low-dose TIV/Advax® induced efficient immune response	Phase I	2016
		Tetanus	Toxoid vaccine (TT)	enhanced mucosal immune response	-	2014
		Influenza	Subunit vaccine (HA-split)	enhanced humoral and cell-mediated immune responses	-	2014
		various	various	Th1 polarization	-	2015
		various	various	Th1 polarization	clinical study (newborn)	2016

Human

Vaccine Type	Vaccine Target	Product Name	Administration	Date of Approval	Company involved
Live attenuated vaccine	Cholera	Vaxchora®	Oral	2016	PaxVax
	Influenza	FluMist®	Intranasal	2003	MedImmune
Inactivated vaccine	Influenza virus subtypes A and type B	Flucelvax®	Intramuscular	2012	Novartis
	Influenza	Fluzone®	Intradermal	2002	Sanofi Pasteur
inactivated Hepatitis A and recombinant protein	Hepatitis A and B	Twinrix®	Intramuscular	2001	GlaxoSmithKline
	Invasive meningococcal disease	Menveo®	Intramuscular	2010	Novartis
Toxoid conjugated vaccine	Haemophilus influenzae type b	Hiberix®	Intramuscular	2009	GlaxoSmithKline
	Diphtheria, Tetanus, Acellular Pertussis, Hepatitis B, Polio	Pediarix®	Intramuscular	2002	GlaxoSmithKline
Polysaccharide vaccine	Streptococcus pneumoniae	Prenar 13®	Intramuscular	2010	Wyeth
Recombinant proteins	Meningococcal Group B	Bexsero®	Intramuscular	2015	Novartis
	Influenza virus subtypes A and type B	Flublok®	Intramuscular	2013	Protein Science

Animal

Vaccine Type	Vaccine Target	Product Name	Species	Date of Approval	Company involved
DNA vaccine	West Nile virus	West Nile-Innovator®	Horses	2005	Fort Dodge
	Infectious haematopoietic necrosis virus (IHNV)	Apex-IHN®	Salmon	2005	Novartis
	Growth hormone releasing hormone (GHRH)	LifeTide® SW5	Swine	2008	VGX™ Animal Health
	Melanoma	Oncept™	Dogs	2010	Meril

<u>Human</u>	Product name	Vector name	Vaccine formulation	Delivery method	Clinical status	Trial number	Sponsor
DNA vaccine priming only							
	PENNVAX®-B	--	DNA vaccine	CELLECTRA intramuscular electroporation device	Phase I	NCT01082692	Inovio Pharmaceuticals
HIV infection (Prophylactic vaccine)							
	PENNVAX®-GP	--	DNA vaccine + plasmid cytokine adjuvant (IL-12)	Intradermal injection/ intramuscular injection with CELLECTRA® electroporation	Phase I	NCT02431767	Inovio Pharmaceuticals
Malaria (Prophylactic vaccine)	EP-1300		DNA vaccine	Intramuscular injection with electroporation via TriGrid™ Delivery System (TDS)	Phase I	NCT01169077	KAEL-GemVax
Hepatitis B (Therapeutic immunotherapy)	INO-1800®	--	DNA vaccine + plasmid cytokine adjuvant (IL-12)	CELLECTRA® electroporation device	Phase I	NCT02431312	Inovio Pharmaceuticals
Zika virus infections (Prophylactic vaccine)	GLS-5700®	pGX7201	DNA vaccine only	Intradermal injection with CELLECTRA® electroporation	Phase I	NCT02809443 NCT02887482	GeneOne Life Science Inovio Pharmaceuticals
Middle East respiratory syndrome coronavirus (MERS CoV) (Prophylactic vaccine)	GLS-5300®	--	DNA vaccine only	Intramuscular injection with CELLECTRA® electroporation	Phase I	NCT02670187	GeneOne Life Science Inovio Pharmaceuticals
Influenza A H5N1 and H1N1 subtypes (Prophylactic vaccine)	INO-3510®	--	DNA vaccine only	Intradermal injection with CELLECTRA® electroporation	Phase I	NCT01405885	Inovio Pharmaceuticals
Viral hemorrhagic fever with renal syndrome (Prophylactic vaccine)	HTNV/PUUV DNA Vaccine	pWRG/HTN- M(co)/pWRG/ PUUV-M(s2)	DNA vaccine only	Intramuscular injection with electroporation via TriGrid™ Delivery System (TDS)	Phase II	NCT02116205	Ichor Medical Systems US Army Medical Research and Materiel Command
Cytomegalovirus infection in hematopoietic cell transplantation/solid organ (kidney) transplantation	ASP0113	TransVax	DNA vaccine with poloxamer-based CRL1005 delivery system	Intramuscular injection	Phase III (Results did not meet expected criteria, announced on Jan 22, 2018)	NCT01877655 NCT01974206	Astellas Pharma Vical
HSV-2 infection (Therapeutic vaccine)	herpes simplex bivalent DNA vaccine	VCL-HB01	DNA vaccine only	Intramuscular injection	Phase II	NCT02837575	Vical
DNA vaccine priming and other vaccine boosting							
HIV infection (Prophylactic vaccine)	GOVX-B11	pGA2/JS7	DNA vaccine prime+ MVA vaccine boost	Intramuscular injection	Phase II	NCT00820846	GeoVax
HIV infection (Prophylactic vaccine)	PENNVAX®-G	--	DNA vaccine prime+ MVA-CMDR vaccine boost	Intramuscular delivery by Biojector 2000® needleless device/CELLECTRA intramuscular electroporation device	Phase I	NCT01260727	Inovio Pharmaceuticals
Malaria (Prophylactic vaccine)	--	--	DNA vaccine prime+ adenovirus type 5 vaccine (Ad) boost	Intramuscular delivery by Biojector 2000® needleless device	Phase I/IIa	NCT00870987	Vical, U.S. Army Medical Research and Materiel Command

Statement of Significance

This review paper summarizes the state of the engineered/recombinant DNA vaccine field, with a scope entailing “Engineering DNA vaccines against infectious diseases”. We endeavor to emphasize recent advances, recapitulating the current state of the field. In addition to discussing DNA therapeutics that have already been clinically translated, this review also examines current research developments, and the challenges thwarting further progression. Our review covers: recombinant DNA-based subunit vaccines; internalization and processing; enhancing immune protection via adjuvants; manufacturing and engineering DNA; the safety, stability and delivery of DNA vaccines or plasmids; controlling gene expression using plasmid engineering and gene circuits; overcoming immunogenic issues; and commercial successes. We hope that this review will inspire further research in DNA vaccine development.